

1. MRI with inclined field.

- (a) Show that the MRI with an inclined field, $\mathbf{B}_0 = (0, B_{0y}, B_{0z})$ and a spatial dependence of all variables only in the z direction is given by the following eigenvalue problem:

$$\begin{pmatrix} \sigma & -2\Omega & 0 & 0 & -ik\frac{B_{0z}}{\mu_0\rho_0} & 0 \\ S + 2\Omega & \sigma & 0 & 0 & 0 & -ik\frac{B_{0z}}{\mu_0\rho_0} \\ 0 & 0 & \sigma & ikc_s^2 & 0 & ik\frac{B_{0y}}{\mu_0\rho_0} \\ 0 & 0 & ik & \sigma & 0 & 0 \\ -ikB_{0z} & 0 & 0 & 0 & \sigma & 0 \\ 0 & -ikB_{0z} & ikB_{0y} & 0 & -S & \sigma \end{pmatrix} \begin{pmatrix} \hat{u}_{x1} \\ \hat{u}_{y1} \\ \hat{u}_{z1} \\ \hat{\rho}_1/\rho_0 \\ \hat{B}_{x1} \\ \hat{B}_{y1} \end{pmatrix} = 0. \quad (1)$$

- (b) Expand the matrix governing the eigenvalue problem and discuss the solutions. To simplify the notation, define the two Alfvén frequencies $\omega_{Ay}^2 = k^2 v_A^2$ and $\omega_{Az}^2 = k^2 v_A^2$, with $v_A^2 = B_{0z}^2/(\mu_0\rho_0)$ and v_A being the Alfvén velocity. as well as the acoustic frequency $\omega_c^2 = k^2 c_s^2$. Begin by discussing special cases: verify that the usual MRI solution is recovered for $B_{0y} = 0$.
- (c) Next, discuss $B_{0y} \neq 0$ and either (i) $B_{0z} = \Omega = S = 0$, (ii) $\Omega = S = 0$ with $B_{0z} \neq 0$, (iii) $S = 0$ with $\Omega \neq 0$ and $B_{0z} \neq 0$, and finally the case (iv) in which neither S , Ω , nor B_{0z} vanish,
- (d) Compute solutions of the full problem numerically. Plot first σ^2 as a function of the inclination θ of the field $\mathbf{B}_0 = B_0(0, \sin\theta, \cos\theta)$ for $\Omega = S = 0$ and $c_s = 1$ and (i) $v_A = 0.7$, (ii) $v_A = 1$, (iii) $v_A = 2$.

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- (a) In the presence of rotation and shear, the MHD equations for the departure from the shear flow \mathbf{u} , the magnetic field \mathbf{B} , and the density ρ becomes

$$\frac{\partial \mathbf{u}}{\partial t} + Sx \frac{\partial \mathbf{u}}{\partial y} + u_x S \hat{\mathbf{y}} + \mathbf{u} \cdot \nabla \mathbf{u} + 2\Omega \times \mathbf{u} = -\rho^{-1} \nabla P + \rho^{-1} \mathbf{J} \times \mathbf{B}, \quad (2)$$

$$\frac{\partial \mathbf{B}}{\partial t} + Sx \frac{\partial \mathbf{B}}{\partial y} + \mathbf{u} \cdot \nabla \mathbf{B} = B_x S \hat{\mathbf{y}} + \mathbf{B} \cdot \nabla \mathbf{u} - \mathbf{B} \nabla \cdot \mathbf{u}, \quad (3)$$

$$\frac{\partial \rho}{\partial t} + Sx \frac{\partial \rho}{\partial y} + \mathbf{u} \cdot \nabla \rho = -\rho \nabla \cdot \mathbf{u}. \quad (4)$$

Let us here, for simplicity, consider an isothermal equation of state, i.e., $P = \rho c_s^2$, where $c_s = \text{const}$. The equations can be readily linearized about $\mathbf{u} = 0$, $\mathbf{B} = \mathbf{B}_0 = \text{const}$, and $\rho = \rho_0 = \text{const}$. For the following, we assume $\mathbf{B}_0 = (0, B_{0y}, B_{0z})$ and $\nabla = (0, 0, \partial_z)$. We assume that all perturbations are proportional to $e^{\sigma t + ikz}$. Thus we have

$$\begin{pmatrix} \sigma & -2\Omega & 0 & 0 & -ik\frac{B_{0z}}{\mu_0\rho_0} & 0 \\ S + 2\Omega & \sigma & 0 & 0 & 0 & -ik\frac{B_{0z}}{\mu_0\rho_0} \\ 0 & 0 & \sigma & ikc_s^2 & 0 & ik\frac{B_{0y}}{\mu_0\rho_0} \\ 0 & 0 & ik & \sigma & 0 & 0 \\ -ikB_{0z} & 0 & 0 & 0 & \sigma & 0 \\ 0 & -ikB_{0z} & ikB_{0y} & 0 & -S & \sigma \end{pmatrix} \begin{pmatrix} \hat{u}_{x1} \\ \hat{u}_{y1} \\ \hat{u}_{z1} \\ \hat{\rho}_1/\rho_0 \\ \hat{B}_{x1} \\ \hat{B}_{y1} \end{pmatrix} = 0. \quad (5)$$

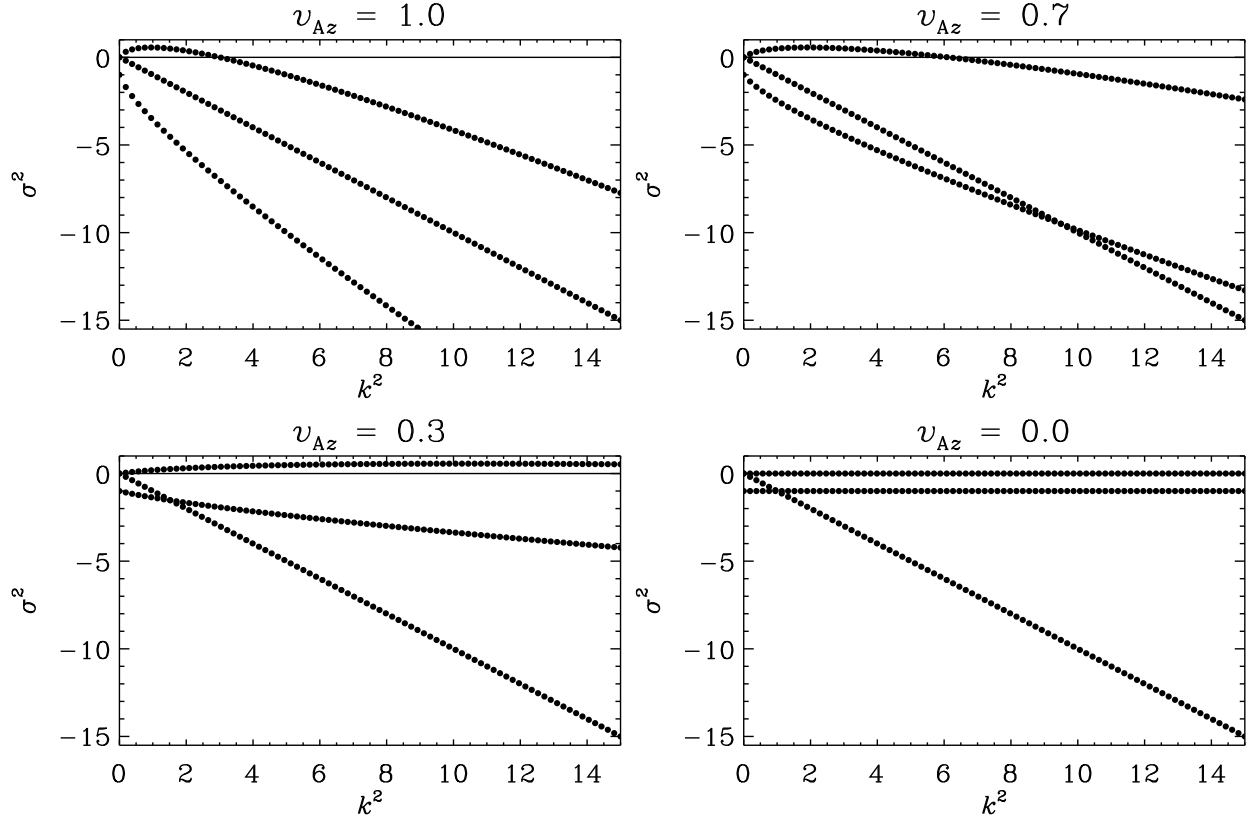


Figure 1: Starting from the usual MRI case (here $\Omega = 1$, $S = -3/2$, $v_{Ay} = 0$ and $c_s = 1$), we see that for decreasing v_{Az} the lower (fast magnetosonic) branch becomes essentially flat and turns into what is called an inertial mode with $-\sigma^2 = \Omega$. The slow magnetosonic branch also becomes essentially flat, but with zero frequency.

Requiring the determinant to vanish yields the dispersion relation as

$$\sigma^6 + \sigma^4[\omega_c^2 + \omega_{Ay}^2 + 2\omega_{Az}^2 + 2\Omega(S + 2\Omega)] \quad (6)$$

$$+ \sigma^2 \left[2\Omega(S + 2\Omega)(\omega_c^2 + \omega_{Ay}^2) + \omega_{Az}^2(2\omega_c^2 + \omega_{Ay}^2 + \omega_{Az}^2 + 2\Omega S) \right] \quad (7)$$

$$+ \omega_c^2 \omega_{Az}^2 (\omega_{Az}^2 + 2\Omega S) = 0 \quad (8)$$

- (b) We already know that for $v_{Ay} = 0$, the soundwaves decouple. In that case the full MRI, as discussed in Handout 2, is recovered. In Fig. 1 we see the dispersion relation for different values of v_{A0} . This case is interesting, because the Alfvén and fast magnetosonic modes cross at a certain value of k .
- (c) For $v_{Ay} \neq 0$, however, soundwaves no longer decouple. An important limit is $\Omega = S = 0$, in which case we can write

$$\sigma^6 + \sigma^4(\omega_c^2 + \omega_{Ay}^2 + 2\omega_{Az}^2) + \sigma^2 \omega_{Az}^2 (2\omega_c^2 + \omega_{Ay}^2 + \omega_{Az}^2) + \omega_c^2 \omega_{Az}^4 = 0. \quad (9)$$

Inspecting again Eq. (5), we see that the first and fifth row and column collapse into an independent matrix whose determinant must vanish, i.e.

$$\det \begin{pmatrix} \sigma & -ik \frac{B_{0z}}{\mu_0 \rho_0} \\ -ik B_{0z} & \sigma \end{pmatrix} = 0, \quad (10)$$

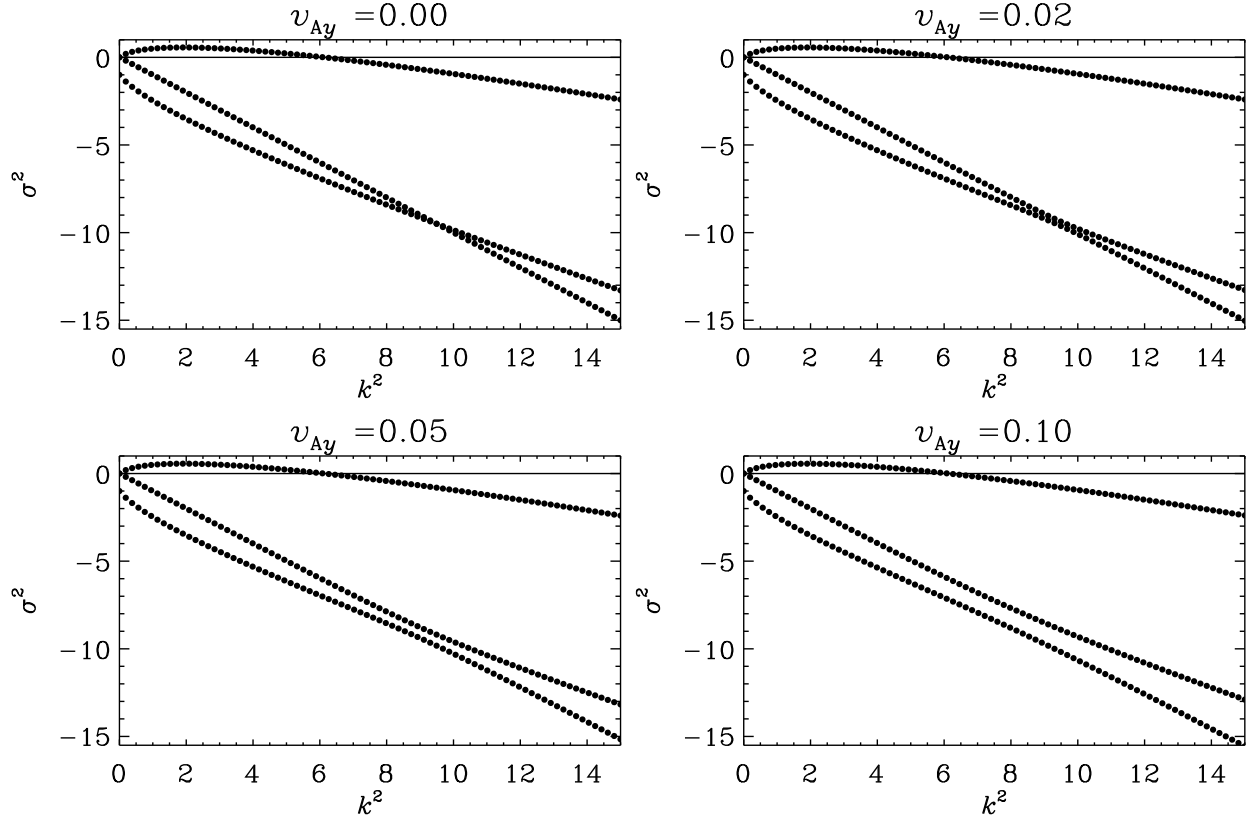


Figure 2: MRI case (again with $\Omega = 1$, $S = -3/2$, and $c_s = 1$), but now with $v_{Az} = 0.7$ and 4 values of v_{Ay} . Note the appearance of *avoided crossings*.

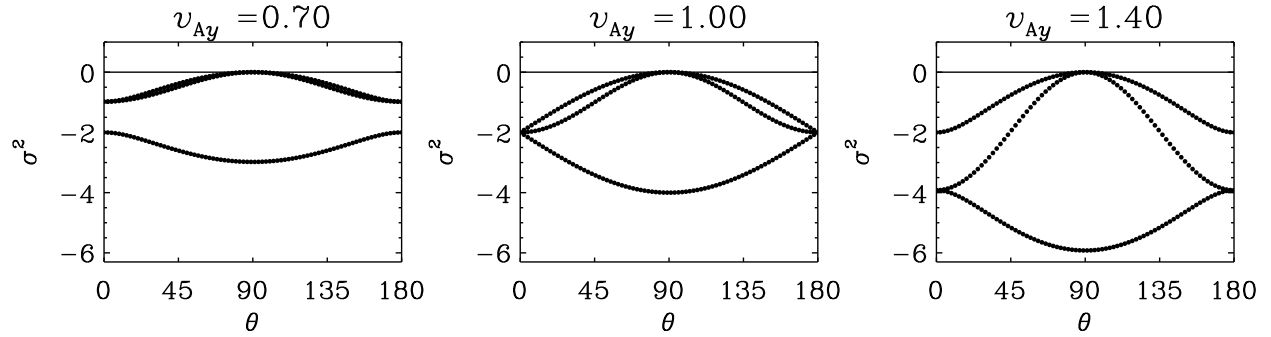


Figure 3: Dependence on θ for $\Omega = S = 0$, $c_s = 1$, and three values of v_A .

so the dispersion relation reads

$$(\sigma^2 + \omega_{Az}^2) \left[\sigma^4 + \sigma^2(\omega_c^2 + \omega_{Ay}^2 + \omega_{Az}^2) + \omega_{Az}^2 \omega_c^2 \right] = 0 \quad (11)$$

Note that the sound and fast magnetosonic branches *cross*; see Fig. 1. For finite values of v_{Ay} , these branches no longer cross. In such a case, one often talks about *avoided crossings*. The onset of MRI is not affected, however; see Fig. 2.

(d) We now consider the dependence on θ . Fig. 3 shows the three modes for $\Omega = S = 0$.

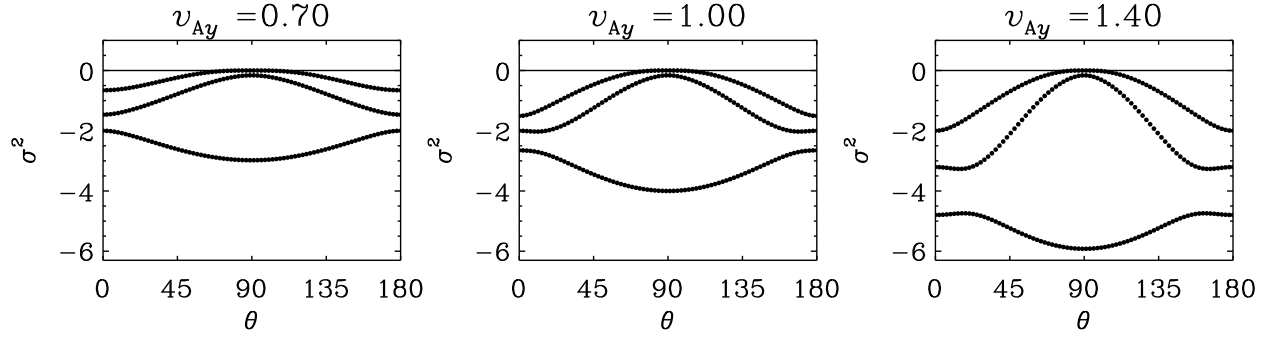


Figure 4: Similar to Fig. 3, but for $\Omega = 0.2$. Note that now the degeneracy between Alfvén and magnetosonic modes is lifted even for the fast magnetosonic modes at $\theta = 0^\circ$ and the slow magnetosonic modes at $\theta = 90^\circ$.

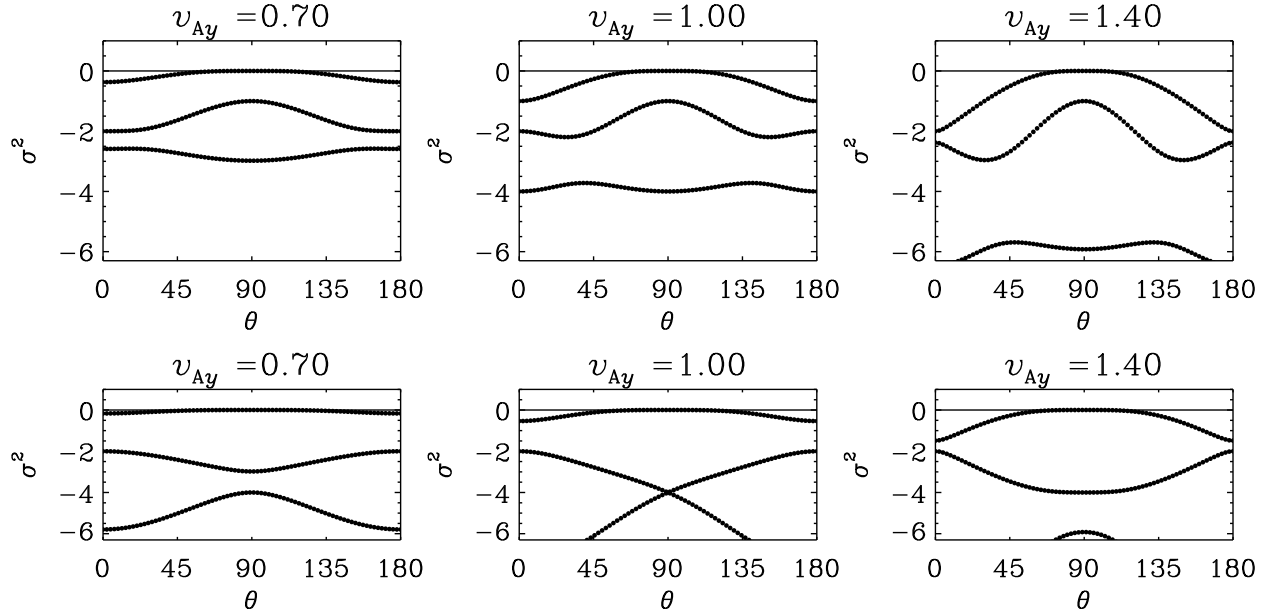


Figure 5: Similar to Fig. 3, but for $\Omega = 0.8$ (upper row) and $\Omega = 1$ (lower row). Note the dramatic changes between these two cases.

Note that the degeneracy between Alfvén and magnetosonic modes is lifted, except for the fast magnetosonic modes at $\theta = 0^\circ$ and the slow magnetosonic modes at $\theta = 90^\circ$.

For finite values of vAy , the degeneracy between Alfvén and magnetosonic modes is lifted even for the fast magnetosonic modes at $\theta = 0^\circ$ and the slow magnetosonic modes at $\theta = 90^\circ$; see Fig. 4. As we increase the value of Ω , the θ dependence changes dramatically between all these cases; see Fig. 5. Finally, for finite shear, we see the emergence of MRI for certain angles; see Fig. 6.

2. Compute numerically the solutions of the anharmonic oscillator

$$\ddot{x} = -\sin x \tag{12}$$

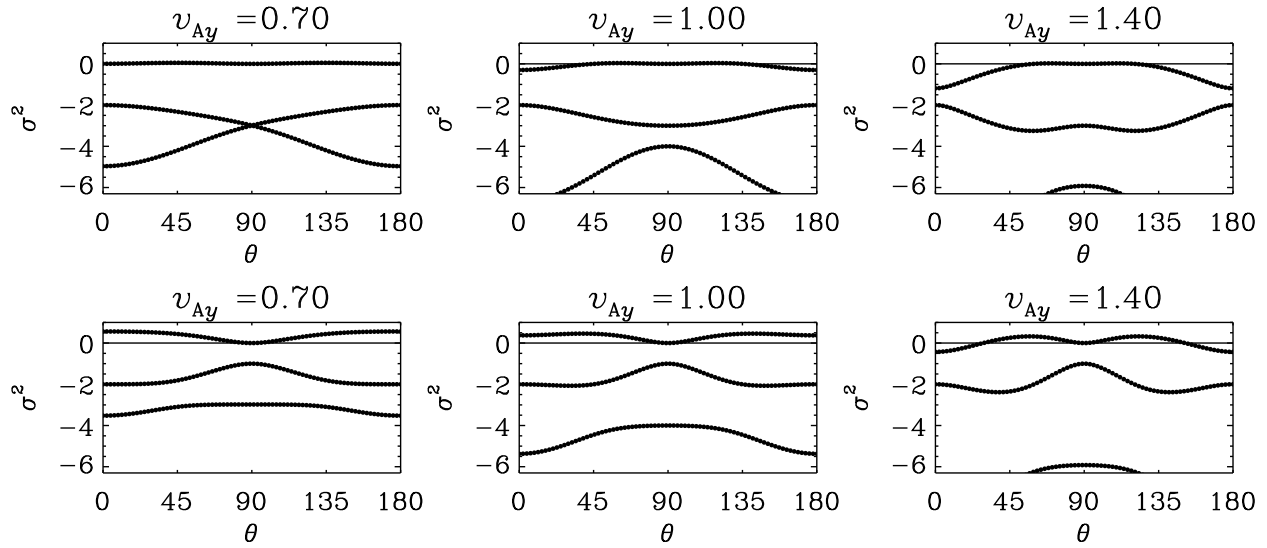


Figure 6: Similar to Fig. 5, but for $\Omega = 1$ and $S = -0.5$ (upper row) and $S = -1.5$ (lower row).

both as $x(t)$ and $\dot{x}(t)$, but also, for a set of different initial conditions, as parametric plots, in the plane $x(t)$ vs $\dot{x}(t)$.

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 Let me show you here the very nice illustration by Michelle Maiden in Figs. 7 and 8.

3. Compute the eigenfrequencies of the Rayleigh-Benard problem with free-slip boundary conditions and negative values of Ra for parameters of your choice. Explain in words the physical difference between positive and negative values of Ra.

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 See Fig. 9. For negative Ra, there are only oscillatory solutions that correspond to Brunt-Väsälä oscillations; see Fig. 9.

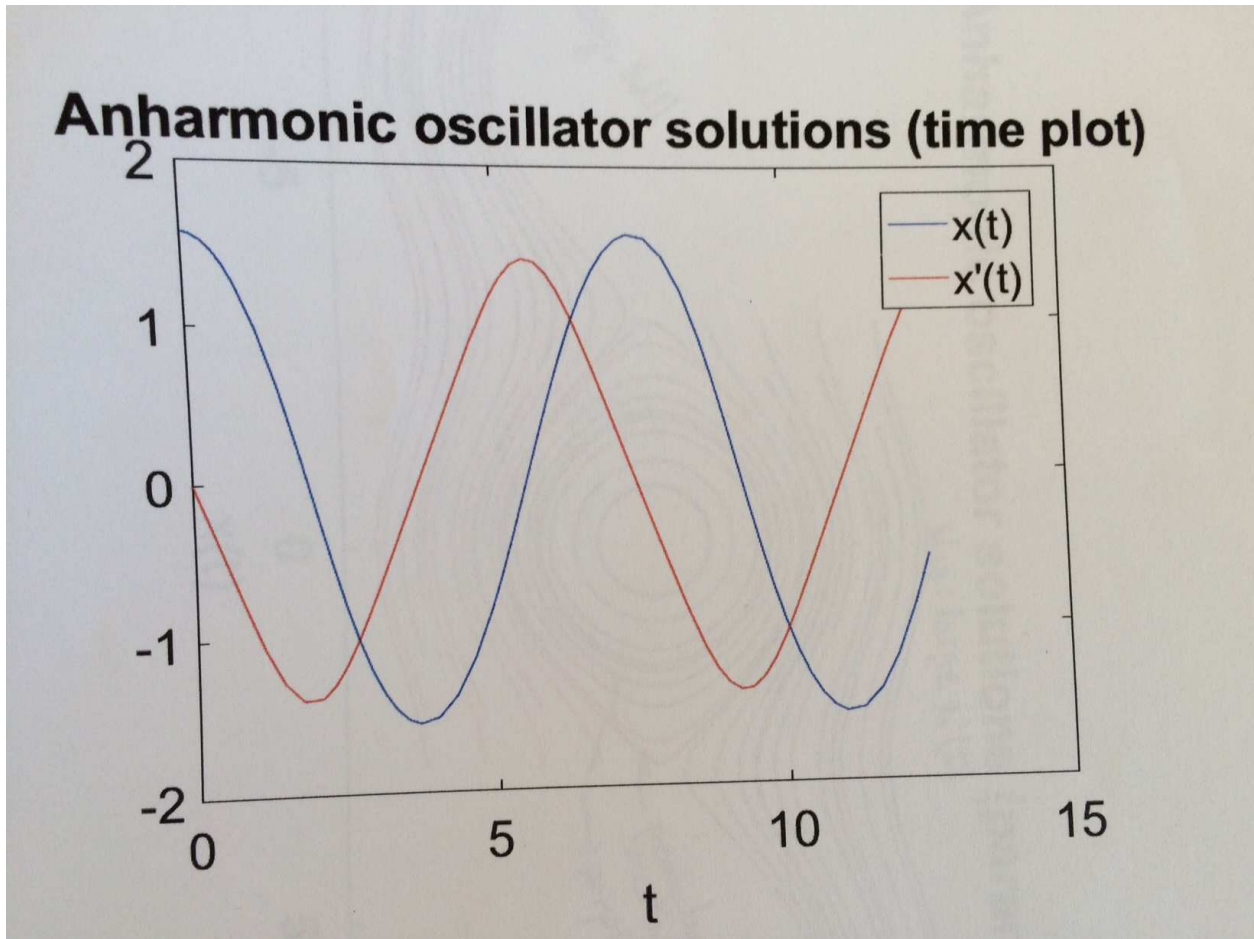


Figure 7:

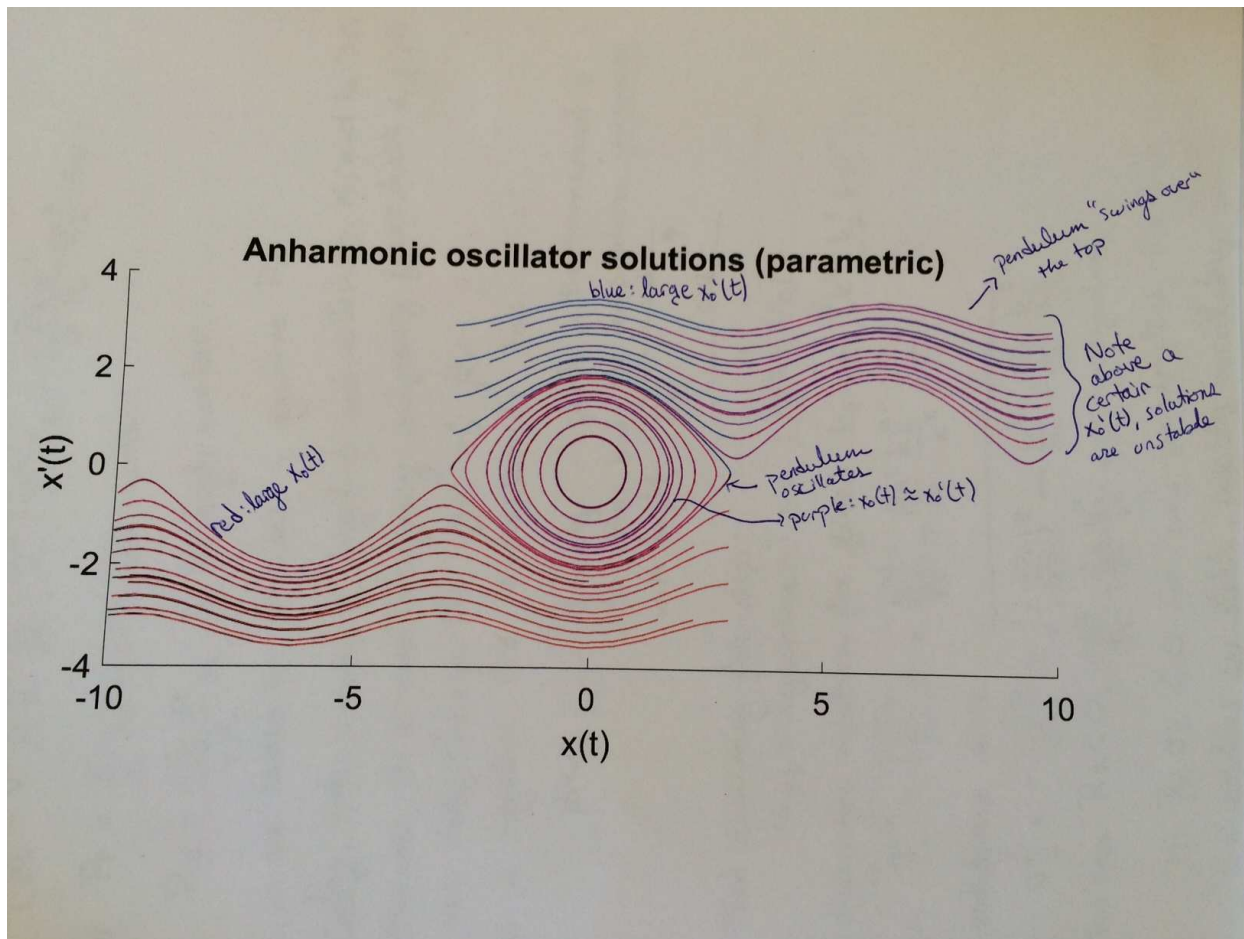


Figure 8:

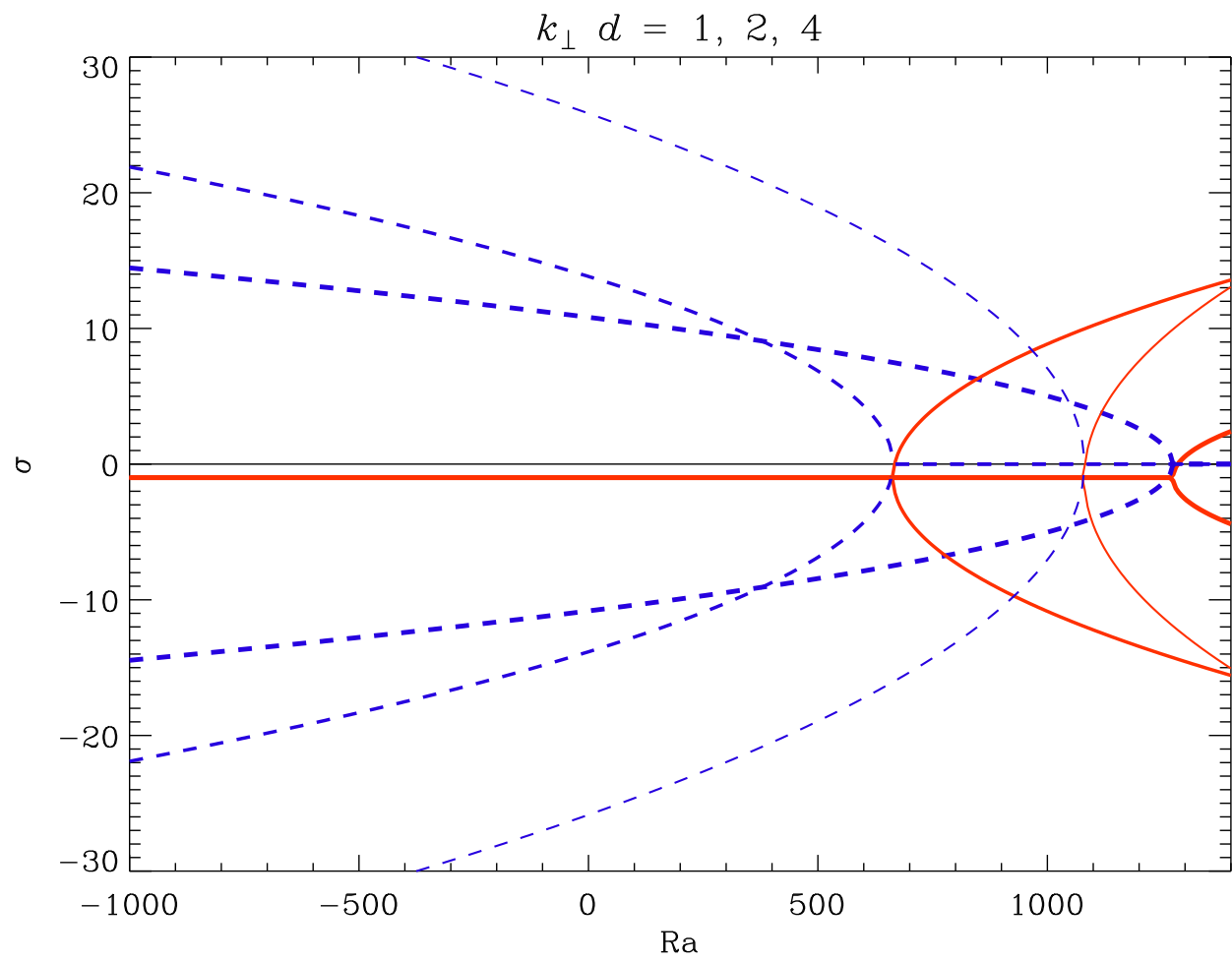


Figure 9: Similar to the plot in Handout 3.